

**REMARKS:**

The present Amendment makes editorial changes in the title,  
specification, drawings and claims, and adds an Abstract, to conform the  
5 present PCT application to the requirements of United States patent practice  
and to direct the specification and the claims solely to a method.

Early consideration of the application is respectfully requested.

Submitted by,

*Steven H. Noll* \_\_\_\_\_ (Reg. 28,982)

10 Schiff, Hardin LLP  
**CUSTOMER NO. 26574**  
Patent Department  
6600 Sears Tower  
233 South Wacker Drive  
Chicago, Illinois 60606  
Telephone: 312/258-5790  
15 Attorneys for Applicant(s).

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COMPUTED TOMOGRAPHY APPARATUS COMPRISING A FADE-IN DEVICE AT THE Emitter END, AND METHOD FOR OPERATING SUCH A COMPUTED TOMOGRAPHY APPARATUS

SPECIFICATION

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TITLE"METHOD FOR OPERATING A COMPUTED TOMOGRAPHY APPARATUS HAVING A DIAPHRAGM AT THE RADIATION DETECTOR"BACKGROUND OF THE INVENTIONField of the Invention

10 The present invention concerns a method for operating a computed computer tomography apparatus with an x-ray radiator rotatable around a system axis, with an x-ray detector and with a radiator-side gating device that comprises has two opposite absorber elements that can be adjusted in a straight line, in particular that can be adjusted with regard to their separation from one another,

15 for variable delimitation of the ray beam. The invention also concerns a method for operation of such a computer tomography apparatus, in which an An examination subject is scanned under during rotation of the x-ray radiator and by means of a translatory relative translational movement between the x-ray radiator and the examination subject in the direction of the system axis.

20 Description of the Prior Art

In an examination of an examination subject or a patient in an x-ray diagnostic apparatus, the examination subject is inserted moved into an x-ray beam emitted by an x-ray source, and the radiation attenuation resulting from this actuated by the subject is detected by an x-ray detector. The examination subject is thus located in the beam path between the x-ray receiver source and the x-ray detector. The typical x-ray tubes used as x-ray radiators emit radiate x-ray radiation in a significantly larger solid angle than is necessary for examination at the patient. In order to prevent an unnecessary radiation exposure at the patient, the necessity thus exists to gate out unnecessary x-rays are gated (blanked out).

30 For this, in conventional x-ray apparatuses it is known to apply dispose a radiator-

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side gating device immediately after the x-ray radiator in the beam path, which. Such gating device is also designated as a primary beam diaphragm. For example, such a primary beam diaphragm, with diaphragm plates which that can be moved opposite to one another as absorber elements, is known from EP-0-187

5 245-A1 European Application 0 187 245.

In computer computed tomography apparatuses with multi-row x-ray detectors, a detector-side beam diaphragm (or a beam diaphragm near to the detector) that is mounted in the beam path between the patient and the x-ray detector is also frequently used in addition to a radiator-side gating device that is 10 arranged in the beam path between the x-ray radiator and the patient. It is thereby possible to shade shadow one or more detector rows of the plurality of multiple detector rows present and to use the remaining detector rows as active detector rows. Since, in a computer tomography apparatus (in particular in such a computer tomography apparatus of the third generation), the x-ray detector 15 rotates around the patient together with the x-ray radiator mounted on a gantry (rotating frame), the control and/or regulation device is normally curved in the azimuthal direction. In adaptation to this geometry, in particular in order to realize a constant separation, a detector-side diaphragm disclosed in DE 42 26 861 C2 for a computer tomography apparatus is fashioned with arc-shaped diaphragm 20 plates.

With regard to the radiator side diaphragm, the objective exists that this only passes such rays which can also actually be detected by the x-ray detector (and in particular by its active detector rows). Other x-rays would only unnecessarily penetrate the patient and unnecessarily increase the radiation 25 exposure. Since the multi-row x-ray detector arrays in computer tomographs are normally equipped with orthogonal rows and columns of detector elements, with regard to the primary beam diaphragm the objective exists to gate an exactly rectangular ray beam. Given flat or planar diaphragm plates or absorber elements, this is not perfectly possible due to different separations of the x-rays of 30 the ray beam, respectively measured from the focus of the x-ray radiator to the

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point of impact on the diaphragm plate. To prevent corresponding disadvantageous edge effects in the gating, in US 6,396,902 B2 an x-ray collimator is specified in which a plurality of slits of different but respectively constant width are introduced in a carrier or base body, whereby the carrier body  
5 is curved such that the gating slits are also curved. Via the curvature of the slits, it should be ensured that a ray beam exactly rectangular in cross section is gated on the x-ray detector.

For different examination methods, in order to be able to operate with different numbers of active detector rows or with an x-ray beam gated at different  
10 widths in the direction of the patient axis, given the x-ray

Such a collimator is known from US United States Patent No. 6,396,902 B2 the entire bearing body produced from composed of x-ray-absorbing material must be moved. According to the local disclosure, this This occurs via by rotation of the bearing body, which is why the bearing body is also curved around a  
15 second axis. In order to thereby also be able to bring another diaphragm slit into the matching position, the rotation axis would have to be located at the height of the focus of the x-ray radiator. This is at best possible with very large mechanical effort.

Alternatively, the rotated bearing body would have to be readjusted into the  
20 correct position via a shifting movement, which is likewise very elaborate. Moreover, the production of a bearing body curved around two axes is expensive likewise connected with large expenditure, whereby because this must also still be produced from x-ray-absorbing material, meaning from a material with a high atomic number.

25 Moreover, what is disadvantageous from A further disadvantage of the x-ray collimator known from US United States Patent No. 6,396,902 B2 is that only a finite number of slits of discrete width can be applied or, respectively, introduced on or in the bearing body.

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The invention is based on the object to specify a computer tomography apparatus with a radiator-side gating device which exhibits more flexible gating possibilities and which can be simultaneously be produced with less expenditure. A method for operation of such a computer tomography apparatus should also be  
5 specified.

The object with regard to the apparatus is achieved according to the invention with regard to the computer tomography apparatus cited above in that the absorber elements exhibit a curved shape, and that the gating device comprises an adjustment device that acts on the absorber elements such that the  
10 absorber elements can be moved perpendicular to their longitudinal direction, in particular can be adjusted [displaced] relative to one another. The elements can in particular be moved in a direction parallel to the system axis. The absorber elements exhibit the curved shape in particular on their outer contour delimiting the x-ray beam, i.e. for example on an edge forming a diaphragm slit.

15 The inventive computer tomography apparatus has the advantage that the slit width is continuously or freely selectable between the curved absorber elements or diaphragm jaws [cheeks], and thus the slice thickness adjustable at the computer tomography apparatus can also assume non-discrete values. Wide detector rows can also be only partially irradiated, and thus slices that are thinner  
20 than the width of the detector elements are also possible in a simple manner.

Moreover, the gating device of the inventive computer tomography apparatus requires absorber elements that are necessarily curved only in one direction or in one plane and that thus exhibit, for example, a shape as is created given bending of a plate around a straight edge (for example "banana shape").  
25 The gating device can thus also be produced simply.

The variation, continuous to the greatest possible extent, of the slit width or the collimation width possible in the computer tomography apparatus according to the invention allows as already mentioned a free selection of the slice thickness and a flexible selection of the active rows of detector elements.

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However, a readjustment of the diaphragm setting given a change of the focus size in the x-ray receiver occurring during the operation is moreover also still possible.

According to a preferred embodiment, the absorber elements can be moved independent of one another. It is therewith in particular possible to move the absorber elements not only opposite one another, but rather also concurrently in one and the same direction. For example, a diaphragm readjustment is thereby also possible given a variation of the focus position in the diaphragm rays occurring during the operation (focal spot tracking). This means that the entire slice can also be shifted in the z direction with a constant slice width. Moreover, a dynamic variation of the collimation width is therewith possible, whereby (for example) an unwanted over radiation at the beginning and at the end of a spiral scan can be reduced, in that one of the absorber elements is still closed at the beginning of the scan and is only opened at the beginning of the scan with the beginning of the translatory patient bed movement in the direction of the system axis. The same is correspondingly true in reverse for the end of the scan.

The adjustment device for each of the absorber elements comprises a separate adjustment means, whereby the adjustment means are preferably fashioned for a linear movement of the appertaining absorber element. Via such a linear movement, it is ensured in an advantageous manner that sections of the curved absorber element matching one another also still lie opposite one another after a relative movement in the direction of the system axis.

With particular advantage, the adjustment means comprise a (preferably mutual) linear guide as well as, respectively, a drive means [actuator] acting on the absorber elements.

As an alternative to this, the adjustment means respectively comprise a linear meter, for example with a corresponding respective guide.

The curvature of the absorber elements runs in particular in a plane perpendicular to the system axis. The curvature in particular exhibits the shape of

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a circular arc whose center point lies in the focus of the x-ray radiator. Identical distances between the focus and all ray-delimiting edge regions of the absorber elements are thereby achieved in a simple manner.

According to another advantageous embodiment, the curvature radii of the  
5 absorber elements differ from one another by a value of 0.5 % to 10 % from the  
interval. The following advantage results from this: in order to enable a hundred-  
percent closure of the diaphragm, due to finishing tolerances it is normally not  
sufficient that the absorber elements contact only on stop [sic]. Rather, they must  
at least slightly overlap, viewed in the direction of the x-ray beam. Such an  
10 overlapping is possible in an advantageous manner without scraping given  
different curvature radii.

The object with regard to the method is achieved according to the invention  
with regard to the method cited above in that, to prevent an unnecessary radiation  
exposure for the examination subject, the gating device is operated with absorber  
15 elements opened to different widths with regard to a center beam of the viewing  
field of the x-ray detector.

It is thereby possible, in particular in an advantageous manner, to prevent  
an over-radiation of the patient at the beginning and at the end of a scan  
movement or a scan (in particular a spiral scan), in that the gating device is  
20 adjusted quasi-asymmetrically.

SUMMARY OF THE INVENTION

An object of the present invention is to provide a method for operating a  
computed tomography apparatus having a beam-gating diaphragm disposed near  
and preceding the radiation detector, wherein over-radiation of the patient at the  
25 beginning and at the end of a scan are avoided.

The above object is achieved in accordance with the present invention in a  
method for operating a computed tomography apparatus wherein the movable

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elements of a beam-gating diaphragm disposed preceding the radiation detector are adjusted in an asymmetrical manner.

According to the invention, this object is achieved by a method for operation of a computed tomography apparatus with a radiator-side gating device  
5 having absorber elements exhibiting a curved shape. The gating device has an adjustment device that acts on the absorber elements such that the absorber elements can be moved perpendicularly to their longitudinal direction, so they can be adjusted (displaced) relative to one another. The elements can be moved in a direction parallel to the system axis. The absorber elements exhibit the curved  
10 shape at their outer contour that delimits the x-ray beam, i.e. for example at an edge forming a diaphragm slit.

To prevent unnecessary radiation exposure for the examination subject, the gating device is operated in accordance with the inventive method with absorber elements opened to different widths with regard to a center beam of the active,  
15 (i.e. radiation detecting) surface of the x-ray detector. This prevents over-radiation of the patient at the beginning and at the end of a scan movement of a scan (in particular a spiral scan), by allowing the gating device to be adjusted quasi-asymmetrically.

For example, before the beginning and/or after the end of the scan  
20 movement, in particular the relative movement, one of the absorber elements is positioned in a closed position and the other absorber element is positioned in an open position.

After the beginning of the scan movement, in particular the relative movement, the absorber element located in the closed position is preferably  
25 opened in sync with the scan movement, in particular with the relative movement.

It is likewise possible that, before the end of the scan movement (in particular the relative movement), one of the absorber elements located in the

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open position is closed in synchronization with the scan movement, in particular with the relative movement.

A dynamic variation of the collimation width is thus effected with the gating device.

5        In an advantageous manner, the slit width is continuously or freely selectable between the curved absorber elements or diaphragm jaws, and thus the slice thickness that is adjustable at the computed tomography apparatus can assume non-discrete values. Wide detector rows can be only partially irradiated, and thus slices that are thinner than the width of the detector elements are also  
10      possible in a simple manner.

Moreover, the gating device requires absorber elements that are necessarily curved only in one direction or in one plane and thus exhibit, for example, a shape as is created given bending of a plate around a straight edge (for example "banana shape"). The gating device can thus also be produced  
15      simply.

The variation that is continuous to the greatest possible extent, of the slit width or the collimation width possible in the computed tomography apparatus allows – as already mentioned – a free selection of the slice thickness and a flexible selection of the active rows of detector elements. However, a  
20      readjustment of the diaphragm setting given a change of the focus size in the x-ray receiver occurring during the operation is still possible.

Since the absorber elements can be moved independently of one another, it is possible to move the absorber elements not only opposite one another, but also concurrently in the same direction. For example, a diaphragm readjustment  
25      is possible given a variation of the focus position in the diaphragm rays that occurs during the operation (focal spot tracking). This means that the entire slice can also be shifted in the z-direction with a constant slice width. Moreover, a dynamic variation of the collimation width is possible, whereby (for example) an unwanted over-radiation at the beginning and at the end of a spiral scan can be

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reduced, by one of the absorber elements remaining closed at the beginning of the scan and only being opened at the beginning of the scan with the beginning of the translational patient bed movement in the direction of the system axis. The same is true in reverse for the end of the scan.

5       The adjustment device for each of the absorber elements indicates a separate adjustment unit, whereby the adjustment units are preferably fashioned for linear movement of the appertaining absorber element. With such a linear movement, it is ensured in an advantageous manner that sections of the curved absorber element matching one another still lie opposite one another after a

10      relative movement in the direction of the system axis.

Each adjustment unit has a (preferably mutual) linear guide as well as a drive acting on the absorber elements.

As an alternative, each adjustment unit can have a linear motor, for example with a corresponding guide.

15      The curvature of the absorber elements proceeds in a plane perpendicular to the system axis. The curvature in particular exhibits the shape of a circular arc whose center point lies in the focus of the x-ray radiator. Identical distances between the focus and all ray-delimiting edge regions of the absorber elements are thereby achieved in a simple manner.

20      According to another embodiment, the curvature radii of the absorber elements differ from one another by a value of 0.5 % to 10 % from the interval. The advantage that results from this is to enable a hundred-percent closure of the diaphragm, because due to finishing tolerances it is normally not sufficient for the absorber elements to cease movement upon coming into contact with stop.

25      Rather, they must at least slightly overlap, viewed in the direction of the x-ray beam. Such an overlapping is possible in an advantageous manner without scraping as a result different curvature radii.

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The invention is subsequently explained in detail using three exemplary embodiments and by means of Figures 1 through 7 (schematic only in part). Thereby shown are:

Fig. 1 in partially perspective, partially block diagram representation, CT  
5 apparatus comprising a gating device according to the invention,

Fig. 2 a known gating device,

Fig. 3 the gating device of the CT apparatus of Figure 1 in a schematic representation, whereby the function of the gating device is illustrated in perspective,

10 Fig. 4 the gating device of Figure 3 according to a first exemplary embodiment in detail,

Fig. 5 the gating device of Figure 3 according to a second exemplary embodiment in perspective representation,

Fig. 6 the gating device of Figure 5 in a cross-section representation, and

15 Fig. 7 the gating device of Figure 3 according to a third exemplary embodiment in detail.

DESCRIPTION OF THE DRAWINGS

Figure 1 schematically illustrates the basic components of a computed tomography apparatus operable in accordance with the inventive method.

20 Figure 2 schematically illustrates the structure and operation of a conventional radiation detector-proximate beam-gating diaphragm.

Figure 3 schematically illustrates the radiation detector-proximate beam-gating diaphragm of the CT apparatus of Figure 1, operable in accordance with the inventive method, in a perspective view.

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Figure 4 is a sectional view through a first embodiment of the diaphragm of Figure 3, operable in accordance with the inventive method.

Figure 5 is a perspective view of a second embodiment of the diaphragm of Figure 3, operable in accordance with the inventive method.

5       Figure 6 is a sectional view of the second embodiment of the diaphragm shown in Figure 5, operable in accordance with the inventive method.

Figure 7 is a perspective view of a third embodiment of the diaphragm of Figure 3, operable in accordance with the inventive method.

**DESCRIPTION OF THE PREFERRED EMBODIMENTS**

10       A CT apparatus of the 3rd third generation is shown in Figure 1 in relevant section. Its measurement data acquisition arrangement comprises includes an x-ray radiator 2 with a gating device 3 positioned in front of it, near the source, and an x-ray detector 5, fashioned as a laminar array of a plurality number of rows and columns of detector elements (one of these is designated with 4 in Fig. 1), with an optional beam diaphragm (not explicitly shown) positioned in front of said the x-ray detector 5, close to the detector 5. For reasons of clarity, in Figure 1 only 4 four rows of detector elements 4 are shown; however, the x-ray detector 5 can comprise have further rows of detector elements 4, optionally also with different widths b.

20       The x-ray radiator 2 with the gating device 3 on the one side and the x-ray detector 5 with its beam diaphragm on the other side are mounted opposite one another on a rotary frame (gantry) (not explicitly shown), such that a pyramidal x-ray beam emitted by the x-ray radiator 2 in the operation of the CT apparatus 1 and gated by the adjustable gating device 3 (the ray beams of which x-ray beam are designated with 8) impinges on strikes the x-ray detector 5. By means of the gating device 3 and, if applicable, by means of the detector proximal detector proximate beam diaphragm, a cross-section of the x-ray beam is thereby adjusted such that only that region of the x-ray detector 5 is uncovered (exposed) that can

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be directly met struck by the x-ray beam. In the operating mode illustrated in Figure 1, this [sic] there are four rows of detector elements that are designated as active rows. If applicable, further existing rows are covered by the detector-proximal detector-proximate beam diaphragm and are therefore not active. The  
5 gating device 3 thereby primarily serves to prevent amounts to the importance [sic] of preventing an unnecessary radiation exposure of the examination subject, in particular a patient, in that by keeping rays that otherwise do not arrive at the active rows are also kept away from the examination subject or patient.

The rotary frame can be displaced in rotation rotated around a system axis  
10 Z by means of a drive unit device (not shown). The system axis Z runs is parallel to the z-axis of a spatial rectangular coordinate system shown in Fig. 1.

The columns of the x-ray detector 5 likewise run proceed in the direction of the z-axis, while the rows (whose width b is measured in the direction of the z-axis and is, for example, 1 mm) run transverse proceed to the system axis Z or,  
15 respectively, and the z-axis.

In order to be able to bring the examination subject, for example the patient, into the beam path of the x-ray beam, a bearing support device 9 is provided that can be shifted parallel to the system axis Z, thus in the direction of the z-axis, and in fact such that a synchronization exists between the rotation  
20 rotational movement of the rotary frame and the translation translational movement of the bearing support device 9 in the sense that with the ratio of translation speed to rotation speed is constant, whereby this. This ratio is adjustable in that by setting a desired value selected for the infeed h of the bearing support device 9 per rotation of the rotary frame.

25 A volume of an examination subject located on the bearing support device 9 can thus be examined in the course of a volume scanning, whereby the. The volume scanning is effected in the form of a spiral scanning scan in the sense that, under during rotation of the rotary frame and simultaneous translation of the bearing support device 9 per rotation of the rotary frame, a plurality number of

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projections is are acquired from various projection directions. Given During the spiral scan scanning, the focus F of the x-ray radiator 2 moves on a spiral track S relatively relative to the bearing support device 9. A sequence scan is also possible as an alternative to this spiral scan.

5       The measurement data, read out in parallel during the spiral scan from the detector elements 4 of each active row of the detector system 5 and corresponding to the individual projections, are subjected to a digital-analog conversion in a data processing unit 10, and are serialized and transferred to an image computer 11 which shows the result of an image reconstruction on a  
10 display unit 16, for example a video monitor.

The x-ray radiator 2, for example an x-ray tube, is supplied with the necessary voltages and currents by a generator unit 17 (optionally likewise mutually rotating). In order to be able to adjust this to the respectively necessary values, a control unit 18 with keyboard 19 that allows the necessary adjustments  
15 is associated with the generator unit 17.

~~The other All~~ operation and control of the CT apparatus 1 also ensues by means of the control unit 18 and the keyboard 19, ~~which is illustrated in that with~~ the control unit 18 is connected with the image computer 11.

Among other things, the number of the active rows of detector elements 4  
20 (and therewith the position the gating device 3 and of the optional detector-proximal detector-proximate beam diaphragm) can be adjusted, for which purpose the control unit 18 is connected with adjustment units 20 or, respectively, and 21 associated with the gating device 3 and the optional detector-proximal detector-proximate beam diaphragm. Furthermore the rotation time that the rotary frame  
25 requires for a complete rotation can be adjusted, ~~which is illustrated in that a by means of the~~ drive unit 22 associated with the rotary frame is being connected with the control unit 18.

~~In Figure 2, it is shown which shows the gating that results given with a known gating device 3A with two separate absorber elements 30A, 31A. Shown~~

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is an x-ray beam with edge rays 8A which that emanates from a focus F of an x-ray radiator 2A.

Both edge rays 8A emanating from the focus F and passing the (in this Figure 2) rear absorber element 30A respectively cover a distance d2 from the 5 absorber element 30A. In contrast to this, the comparable distance d1 in the indicated central ray 36 is less than in the edge rays 8A. This is correspondingly also true for the edge rays on the opposite side of the slit 32A. The result is that an x-ray beam whose outer contour 34A is not rectangular is gated on the x-ray detector 5A with its individual detector elements 4A shown in cross-section. In 10 order to fully illuminate irradiate all detector elements 4A of the detector row (with its width b) illuminated here, the outer contour 34A must be set such that its width B2 at the edge approximately corresponds to the width b of the detector row. As a 15 result of the different distances  $d_1 \neq d_2$ , a larger width B1 of the outer contour 34A of the x-ray beam then results in the middle of the detector row. The portion of the x-ray beam occurring in this barrel-shaped region (here shown exaggerated, but nevertheless disturbing with regard to the radiation dose) is ultimately not used.

The gating device 3 of the CT apparatus 1 according to the invention according to Figure 1 is illustrated in Figure 3 in a schematic representation and perspective view. The gating device 3 comprises has two curved absorber 20 elements 30, 31, between which a slit 32 is formed that can pass the x-rays emanating from the focus F of the x-ray radiator 2. The absorber elements 30, 31 (produced from heavy metal, for example from tungsten and/or from tantalum) are curved in a circular arc, whereby with the middle point of the circular arc lies lying in the focus F of the x-ray radiator 2. It is thereby ensured that the separation, 25 both respective spacings of the edge rays 8 and of a central ray 36 respectively measured from the focus F to the absorber elements 30 (or 31), respectively exhibits exhibit the same value d. In an advantageous manner, it is thereby achieved that this causes the x-ray beam gated on by the x-ray detector 5 exhibits to exhibit in cross-section a rectangular outer contour 34 whose constant width B 30 can be perfectly precisely adapted to the width b of one or more detector rows.

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Both absorber elements 30, 31 can be moved or driven ~~independently~~ independently of one another, ~~in particular also running~~ in parallel or opposite, which is indicated by corresponding double arrows 40, 41 in Figure 3.

In Figure 4, ~~it is shown~~ shows how the gating device 3 (shown only schematically) ~~in the Figure~~ can be accommodated in a common housing 50, together with a filter device 45 with one or more (copper) spectral filters 46 (with drive element 47 belonging to the filter changer) and with a wedge filter 48 serving for the variable attenuation of the x-ray beam. The housing 50 ~~comprises~~ has an entrance opening 51 on the side of the focus F and an exit opening 52 on the opposite side.

Moreover, Figure 4 ~~it is shown that~~ shows a separate adjustment means unit 60 or ~~and~~ 61 is present for each of the absorber elements 30, 31, with which adjustment means 60 or, respectively, 61 the absorber elements 30, 31 can be moved linearly, ~~independent~~ independently of one another. In the exemplary embodiment of Figure 4, the first adjustment means unit 60 for one of the absorber elements 30 ~~comprises~~ includes a first drive means 62 fashioned as a step motor, which ~~drive means~~ 62 acts on one of the absorber elements 30 via a first transmission gear 63 and via a first toothed belt 64. For the other absorber element (31, (not visible in Figure 4), a second drive means 67 (likewise fashioned as a step motor) and a second gear transmission 68 ~~is [sic]~~ are correspondingly present in the second adjustment means unit 61. Both drive means units 62, 67 act (for example via different spindle guides) on the two absorber elements 30, 31 moving linearly in the z-direction on ~~one~~ and the same linear guide 65.

The gating device 3 according to Figure 3 is reproduced shown in Figure 5 in a perspective representation according to a second exemplary embodiment. The special banana-like shape of the diaphragm backs 30, 31 is better visible in Figure 5. Moreover, it ~~results from~~ can be seen in Figure 5 that the common linear guide 65 can ~~comprise~~ have a left-side first track 65A as well as a right-side second track 65B.

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The gating device 3 of Figure 5 is explained again in Figure 6 in a cross-section representation in the z-direction. ~~Therein it is in particular visible In Figure 6 it can be seen~~ that the absorber elements 30, 31 are slightly displaced relative to one another in the height direction y, essentially corresponding to the direction 5 of the radiated x-ray beam, in order to prevent a passage of x-ray radiation (~~conditional upon dependent on~~ finishing tolerances) given a complete closing of the gating device 3.

In order to be able to execute the overlap of the absorber elements 30, 31 without friction, it is advantageous that the curvature radii of the absorber 10 elements are slightly different. For example, these are 197 mm ~~or, respectively,~~ and 200 mm, respectively.

A third exemplary embodiment of the gating device according to Figure 3 is shown in detail in Figure 7. This exemplary embodiment is essentially identical to the exemplary embodiment according to Figure 5, ~~however but~~ differs from this in 15 ~~that both by the respective adjustment means units~~ 60, 61 for the absorber elements 30 ~~or, respectively,~~ and 31 comprise a first linear motor 71 with a guide and a second linear motor 72, likewise with corresponding guide.

Instead of a linear guide, other linear adjustment possibilities can also be used.

With the gating device 3, in connection with a focus-phi-z regulation 20 ~~regulated control, it is possible to correspondingly readjust a make appropriate adjustments to account for variation of the focus position or focus size in the x-ray radiator 2 with regard to in~~ the diaphragm adjustment.

Although modifications and changes may be suggested by those skilled in the art, it is the invention of the inventors to embody within the patent warranted heron all changes and modifications as reasonably and properly come within the scope of their contribution to the art.